

1 **Integrating sex and gender in model simulations of cardiovascular flows: a narrative review**

2 Francesca Maria Susin

3 Cardiovascular Fluid Dynamics Laboratory – Department of Civil, Environmental and Architectural
4 Engineering, University of Padova, Italy

5
6
7
8 *Pre-print version of the paper published in the JOURNAL OF SEX- AND GENDER-
9 SPECIFIC MEDICINE, Issn: 2974-8194.*

10 *All rights reserved.*

11 *Distribution is not allowed even if partial*

12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31

32 **Summary**

33 Gender medicine is providing increasingly abundant evidence of the pivotal role played by sex
34 and gender in the pathophysiology of the human circulatory system¹. Therefore, any medical or
35 nonmedical scientific activity focused on cardiovascular issues must integrate sex and/or gender
36 among the variables that drive blood circulation in order to guarantee the accuracy of the
37 methodological approach, improve the understanding of cardiovascular biomechanical processes,
38 promote a truly personalised medicine, and, last but not least, foster gender equality in healthcare².

39 A preliminary review of the most recent literature in the field of cardiovascular flows (CVF)
40 simulation models is given here, aimed at highlighting if engineering replicas of blood circulation are
41 usually developed according to a gender perspective i.e., if they pay appropriate attention to sex
42 differences and/or gender factors along the entire process of modelling. The proposed examples show
43 that there seems to be a lack of awareness of the basic concepts and alerts spread by gender medicine
44 in the community of cardiovascular flows modellers. Possible reasons and mitigation strategies for
45 such a situation are discussed in the conclusions.

46

47 **Keywords**

48 Cardiovascular Flows Models, Gender Medicine, Gendered Innovation, Engineering Tools, Sex
49 and Gender Analysis, Gender Equality

50

51

52 **1. Cardiovascular flows models**

53 The present section provides some basic information on cardiovascular flows models in order to
54 introduce the reader to the contents of the subsequent sections and allow her or him to better
55 appreciate why engineering studies in the cardiovascular field must be developed according to a
56 gender perspective.

57 Cardiovascular flows models are engineering tools nowadays widely adopted to simulate blood
58 circulation in the human body under healthy and diseased conditions^{3,4}. They replicate the real-world
59 phenomenon (e.g., the flow across the aortic valve) by means of mathematical equations that govern
60 the physics of the problem or in-vitro objects that mimic the anatomy and function of the reproduced
61 system. Whatever their kind i.e., *computational* or *experimental*, CVF models are aimed at
62 quantifying relevant hemodynamic quantities such as blood velocity, flow rate and volumes, pressure
63 waves, pressure gradients, and wall shear stress in the anatomical region under investigation (e.g.,
64 from the left ventricular outflow tract to the ascending aorta) during the entire cardiac cycle.
65 Furthermore, any related hemodynamic index can be calculated from the models' output, e. g. the
66 effective orifice area and the acceleration time in aortic stenosis. Quite recently, moving (e.g. aortic
67 valve leaflets) or deforming (e.g. ascending aorta) boundaries have also been included among
68 elements mimicked in models, to better simulate the real environment. In that case, the behaviour of
69 the solid portion of the system is also part of the models' results (e.g. the geometric aortic valve area
70 in time).

71 In general, CVF models are helpful in the achievement of various goals in the medical and
72 bioengineering areas. They allow a better understanding of the cause-effect relationships in
73 cardiovascular pathophysiology by simulating various scenarios as the diseased condition worsens.
74 For example, Comunale et al.⁵ explored the effect on both pulmonary and systemic circulation of
75 isolated active, passive, and combined right ventricular dysfunction from absent to complete, and
76 their results corroborated the emerging clinical evidence that the filling and pumping efficiency of
77 the right ventricle is far from being less important than that of the left one. The assessment of the
78 hemodynamic performance of medical devices is routinely performed using either computational or
79 experimental models⁶, as also suggested or even required by international standards⁷. As for the
80 clinical practice, both diagnosis and treatment of cardiovascular diseases can greatly benefit from
81 CVF models. For example, in-silico twins might substitute invasive procedures such as cardiac
82 catheterization for the grading of aortic stenosis severity. To this aim, models that calculate the
83 transvalvular pressure gradient at the level of the ascending aorta i.e., after pressure recovery has
84 occurred, have been proposed so far^{8,9}. Note that the latter requires routine echo-Doppler data and

85 thus could be easily adopted in clinical practice. Last but not least, the use of CVF models for surgical
86 planning is rapidly expanding, mainly thanks to the possibility of obtaining an accurate reconstruction
87 of the patient-specific cardiovascular anatomy from medical imaging data¹⁰.

88 It is worth recalling that CVF models can be population- or patient-specific. In the first case, the
89 model replicates a reference subject i.e., an ideal subject that on average represents the investigated
90 population. In the second case, the model is tailored to a specific patient, at least in the limit of clinical
91 data available from that patient. Whatever the case, CVF models usually contain a large number of
92 parameters that describe the anatomy and mechanical response of the cardiovascular functional
93 elements of the modelled subject. To give an example, a model of blood flow in the thoracic aorta
94 will include the size and length of the vessel, the viscosity of blood, the deformability of the aorta,
95 and the cardiac frequency, among other parameters.

96 Finally, accuracy and reliability of models' results are key issues in the field of modelling. They
97 both depend on many factors, which range from purely technical aspects (e. g., the accuracy of
98 measurement instruments or numerical algorithms), to more 'operational' aspects such as the the
99 modeller's experience¹¹, her or his level of knowledge of the pathophysiology of the cardiovascular
100 condition to be replicated, the availability and reliability of the anatomical and functional data
101 required to build the model. However, any CVF model has to be validated before being adopted as a
102 predictive tool. Validation is usually performed by comparing model results mimicking a given real-
103 world scenario (e.g. flow and pressure waves across the healthy aortic valve) and equivalent clinical
104 data. A certain level of mismatch is always present in the comparison, if only because approximation
105 typically affects not only models but also clinical data^{12, 13}. Therefore, the question whether the
106 mismatch is or is not acceptable in essence depends on the expertise and experience of the modeller
107 only.

108

109 **2. Sex and gender in cardiovascular flows modelling**

110 Engineering studies and applications have been considered neutral with respect to sex and gender
111 until recently, when the research on gendered innovations, and a large number of practical case studies
112 spanning from transportation to environmental and, as expectable, biomedical engineering, have
113 shown that they are not¹⁴. In the field of CVF modelling, the reasons and scopes for integrating sex
114 and/or gender among driving variables should be rather intuitive, given the key role played by
115 biological and socio-cultural peculiarities in cardiovascular pathophysiology¹⁵. Nevertheless, the
116 existing CVF modelling literature does not seem to pay adequate attention to sex or gender-related
117 aspects, probably due to the unawareness of the modellers of the issue.

118 In the following subsections, examples from recently published studies are proposed, aimed at
119 pointing out weaknesses of CVF modelling when biological and/or sociocultural diversities among
120 individuals are not taken into account.

121 **2.1 Population-specific CVF models**

122 CVF models have been applied to a large number of cardiovascular conditions common to both
123 sexes so far: healthy, diseased, acquired, congenital, surgically treated, and supported by artificial
124 devices. A quick search on Google Scholar with appropriate keywords can be useful for an example
125 overview.

126 The vast majority of published works develop population-specific models i.e., they should
127 consider, and refer to, a population group unambiguously defined and expected to have a similar
128 circulatory response among the individuals belonging to the group itself. Rather, the description of
129 the mimicked population is often provided in quite a generic or vague way if not left to the reader's
130 interpretation, particularly with respect to the sex. Frequently, modellers refer to "human circulation",
131 "human beings" or even "human-specific models" i.e., without making mention of sexual
132 peculiarities¹⁶ and implicitly assuming that the male and the female circulations, are interchangeable.
133 Further emblematic observations come from the examination of the calibration process i.e., the
134 assignment of realistic values to the parameters that describe the anatomy and the function of the
135 cardiovascular system. In some models, the sex chosen for calibration is not declared at all, although
136 schematic representations of the model domain and/or parameters' values reported in the text allow
137 the reader to presume that a male subject is mimicked¹⁷. However, this might not be true, since it is
138 not uncommon that literature clinical data used to estimate models' parameters were collected from
139 individuals of both sexes, with no differentiation between men and women. In that case, the resulting
140 model twin is neither male- nor female-specific. Some other models are calibrated adopting
141 contemporarily data collected in part from male and in part from female patients¹⁸ i.e., in that case a
142 sort of sex-unspecific circulation is simulated. Finally, when the sex of the reference patient is clearly
143 stated, it is the average adult (Caucasian) man the subject usually considered¹⁹. It is worth noting that
144 in population-specific CVF models not only the calibration but also the validation process typically
145 does not account for sex differences. Again, real data adopted for comparison to model results may
146 refer to samples of male subjects only, both male and female subjects but not differentiated when
147 averaging data, or subjects of unknown/undeclared sex. Finally, population-specific models should
148 be tested with respect to their sensitivity i.e., the variation of models output as an effect of a prescribed
149 variation in parameters values should be calculated. The rationale of the sensitivity analysis is to
150 estimate to what extent the intrinsic uncertainty of calibration affects models predictions, and to
151 highlight the anatomical or functional parameters that mostly affect blood flow properties. As such,

152 the sensitivity analysis can be an excellent tool to give evidence of the role played by sex-related
153 differences in a given cardiovascular condition, provided that parameters values are varied in a range
154 that covers both sexes. However, in models proposed so far the parameters are simply varied of a
155 given percentage around their input value (usually $\pm 10\%$) i.e., no information can be inferred for sex
156 effects.

157 Finally, one may wonder if the sex-specific calibration of population-specific CVF models
158 matters, that is, if sex-specific models are actually capable of reproducing the differences between
159 male and female blood circulation found in clinical research. Indeed, the question is almost
160 unexplored, and to the best of my knowledge, only two contributions have been proposed so far, both
161 focused on the case of healthy young reference subjects^{20, 21}. Models predictions of blood pressures,
162 flow rates and cardiac volumes have been found to differ between the two sexes as expected.
163 Moreover, it has been shown that differences do not vanish when results are indexed with respect to
164 body mass or body surface area i.e., blood circulation in women is confirmed to differ from that in
165 men not only because of the different size. These results corroborate the idea that sex-specific CVF
166 models can greatly contribute to improve the knowledge of the role that sex differences play in
167 cardiovascular pathophysiology. A similar conclusion has recently been reached for what the
168 modelling of cardiac form and function is concerned with²².

169 **2.2 Patient-specific CVF models**

170 Patient-specific models of blood circulation are among the engineering tools that can be of help
171 in the development of the so called personalized medicine i.e., the possibility of tailoring prevention,
172 diagnosis and treatment of diseases on the single individual characteristics. Indeed, recent advances
173 in clinical imaging allow accurate estimation of the anatomical parameters of the examined patient,
174 thus promoting the rapid growth of patient-specific modelling. However, a large number of other
175 functional parameters (e.g., heart chambers elastance) still remain hardly valuable for the patient
176 unless invasive procedures are adopted, and they are rather calibrated starting from cardiovascular
177 data measured in groups of individuals. As a result, calibration of patient-specific models may be
178 affected by the same criticalities highlighted in subsection 2.1. However, the literature shows that
179 both female and male patient-specific models have been proposed so far²³, and in both cases models
180 are inherently sex-specific in a sense, at least in the limit of a sex-specific calibration of relevant
181 parameters²⁴. For what validation is concerned, it is typically performed by comparing model
182 predictions to data measured on the modelled patient himself/herself, and hence the effects of sex
183 peculiarities are inherently, although implicitly, accounted for. However, most of the time the sex of
184 the patient under examination is not recognized as one of the variables that can influence the
185 mimicked circulation, so that model results are analysed and commented without seeking for possible

186 sex-related issues²³. Interestingly, quite a recent work has successfully adopted the patient-specific
187 modelling approach to investigate sex differences in mice hemodynamics²⁵.

188 **2.3 Sex-exclusive cardiovascular conditions in CVF models**

189 Cardiovascular conditions exclusive to one or the other of the two sexes e.g., pregnancy²⁶ and
190 erectile function^{27, 28}, have also been replicated by CVF models. In this case, the first noticeable
191 observation is that sex-exclusive conditions are highly under-represented in the world of
192 cardiovascular flows modelling, with even less attention paid to male than to female circulation. To
193 the best of my knowledge, the works cited above are the only two proposed to investigate
194 cardiovascular issues in erectile dysfunction so far, despite the recognised negative effects on the
195 quality of life of patients due to such a condition. Simulation of blood circulation in pregnant women
196 has received some more attention. Models have been proposed to reproduce hemodynamic changes
197 in healthy pregnancy²⁶, with cardiac chambers²⁹ or vascular³⁰ remodelling eventually taken into
198 account. Cardiovascular conditions that may arise during gestation, e.g. pre-eclampsia³¹, or post-
199 partum, e.g. haemorrhage caused by pernicious placenta previa, have also been investigated³².
200 Importantly, the potential of CVF models as tools capable of assisting cardiologists in predicting pros
201 and cons of pregnancy in women with congenital heart disease starts to be recognized³³.

202 **2.4 Gender and non-binary issues**

203 Clinical research is giving increasing credit to socio-cultural factors as possible determinants of
204 the cause and outcome of cardiovascular diseases². Tako-tsubo syndrome is a good example to refer
205 to, as it seems to be typically associated with the experience of emotional or physical stress as is the
206 case for familiar caregivers, and it affects women much more than men³⁴. However, the biochemical
207 and mechanistic processes that may trigger Tako-tsubo, and their dependence on factors associated
208 with sex, gender, or both, are far from trivial and “easily” detectable, and this circumstance may be
209 one of the reasons why no CVF model of the syndrome has yet been developed.

210 Finally, it is relevant that cardiovascular pathophysiology of neither intersex nor transgender
211 individuals has been the focus of CVF modelling so far. Indeed, at first sight the topic seems to receive
212 little attention also in the clinical research area, which would explain the absence of engineering
213 models.

214

215 **3 Conclusions**

216 An overview of whether and how sex and/or gender are included in engineering models that
217 mimic blood circulation has been proposed. Overall, the main observation that can be inferred from
218 the literature is that modellers are substantially unaware of the role played by both biological and
219 socio-cultural factors in determining the circulatory response in humans.

220 For what sex effects are concerned, models are frequently calibrated adopting sex-unspecific
221 anatomical and functional cardiovascular parameters (that is, obtained from a ‘mixed’ population),
222 and there are cases where the model reference subject presents in part female- and in part male-
223 specific parameters. The same applies to the choice of real cardiovascular data adopted for models
224 validation. It is very possible that such a confused situation is the signal of an insufficient
225 contamination between the clinical sex-specific cardiovascular research and the community of CVF
226 modellers. Therefore, strategic actions aimed at spreading the basic concepts of gender medicine
227 among (bio)engineers have to be reinforced and promoted as much as possible, to foster the birth of
228 the *gender (CVF) engineering*. At the same time, it seems appropriate, if not necessary, that clinical
229 researchers working on sex- and gender-related cardiovascular issues become aware of the existence
230 of CVF models and their enormous potential when built following a sex/gender-specific approach.
231 Dedicated conferences and scientific journals capable of effectively mixing the two communities may
232 be of help. Moreover, journals where CVF models are usually published should adopt editorial
233 policies that ask the reviewers to verify if submitted CVF models pay adequate attention to sex and/or
234 gender. Guidelines detailing the steps required to integrate sex and gender in CVF models have not
235 yet been proposed and seem necessary to that aim.

236 Models that clearly state the sex of the simulated subject(s) consider male patients in most of the
237 cases but attribute the results of simulations to the whole population. This is possibly a consequence
238 of the preferential attention that clinical research itself has historically devoted to male cardiovascular
239 patients. As a result, diagnostic tools, guidelines, and therapeutic strategies and devices, which may
240 benefit from models’ predictions, are at risk of being less accurate for women than for men. However,
241 it should be stressed that, to date, female-specific cardiovascular parameters are only poorly and/or
242 inconsistently present in the clinical literature. Hence, planning and execution of extended
243 cardiovascular parameter data collection campaigns in female samples is paramount, as well as the
244 production of technical guidelines for the consistency of measured data. Technical guidelines should
245 be drawn up by working groups of both engineers and clinicians.

246 Interestingly, it has emerged that some models dedicated to sex-exclusive cardiovascular
247 conditions have been produced. However, they are far less numerous than those that mimic conditions
248 common to both sexes. Furthermore, cardiovascular issues possibly related to gender factors have not
249 attracted CVF modellers so far, as is also the case for blood circulation in intersex and transgender
250 individuals. On the one hand, such a gap may be due to the intrinsic high complexity of the above
251 problems, which are still debated and/or poorly known also in the clinical field. On the other hand, it
252 may be one further signal that minorities are under-represented in the area of health-related research.

253 The present brief review is the first attempt to organically describe the state of the art of CVF
254 modelling from a gender perspective, with the aim of highlighting the current technical,
255 methodological, and ethical criticalities, and providing a first proposal of possible mitigation
256 strategies, actions, and practises.

257

References

- 259 1. Regitz-Zagrosek V, Gebhard C. Gender medicine: effects of sex and gender on
260 cardiovascular disease manifestation and outcomes. *Nat. Rev. Cardiol.* 2022; 1-12.
- 261 2. Reue K, Wiese CB. Illuminating the mechanisms underlying sex differences in
262 cardiovascular disease. *Circ. Res.* 2022; 130(12): 1747-1762.
- 263 3. Maisano F, Redaelli A. Computer modeling of valve disease: a new old technique to
264 understand and predict outcomes. *JACC Adv.* 2022; 1(1): 1-3.
- 265 4. Vardhan M, Randles A. Application of physics-based flow models in cardiovascular
266 medicine: current practices and challenges. *Biophys. Rev.* 2021; 2: 011302.
- 267 5. Comunale G, Peruzzo P, Castaldi B, Razzolini R, Di Salvo G, Padalino MA, Susin FM.
268 Understanding and recognition of the right ventricular function and dysfunction via a
269 numerical study. *Sci. Rep.* 2021; 11(1): 1-12.
- 270 6. Cappon F, Wu T, Papaioannou T, Du X, Hsu PL, Khir AW. Mock circulatory loops used
271 for testing cardiac assist devices: a review of computational and experimental models. *Int.*
272 *J. Artif. Organs* 2021;44(11): 793-806.
- 273 7. Wei ZA, Sonntag SJ, Toma M, Singh-Gryzbon S, Sun W. Computational fluid dynamics
274 assessment associated with transcatheter heart valve prostheses: a position paper of the ISO
275 Working Group. *Cardiovasc. Eng. Techn.* 2018; 9(3): 289-299.
- 276 8. Hatoum H, Mo XM, Crestanello JA, Dasi LP. Modeling of the instantaneous transvalvular
277 pressure gradient in aortic stenosis. *Ann. Biomed. Eng.* 2019; 47(8): 1748-1763.
- 278 9. Susin FM. Complete unsteady one-dimensional model of the net aortic pressure drop. *Op.*
279 *Biomed. Eng. J.* 2019; 13(1).
- 280 10. Govindarajan V, Kolanjiyil A, Johnson NP, Kim H, Chandran KB, McPherson DD.
281 Improving transcatheter aortic valve interventional predictability via fluid–structure
282 interaction modelling using patient-specific anatomy. *Roy. . Open Sci.* 2022; 9(2): 211694.
- 283 11. Melsen LA. It takes a village to run a model - The social practices of hydrological
284 modeling. *Water Resour. Res.* 2022; 58(2): e2021WR030600.
- 285 12. Gallo C, Olbers J, Ridolfi L, Scarsoglio S, Witt N. Testing a patient-specific in-silico model
286 to noninvasively estimate central blood pressure. *Cardiovasc. Eng. Techn.* 2021; 12(2):
287 144-157.
- 288 13. Bonfanti M, Franzetti G, Maritati G, Homer-Vanniasinkam S, Balabani S, Díaz-Zuccarini
289 V. Patient-specific haemodynamic simulations of complex aortic dissections informed by
290 commonly available clinical datasets. *Med. Eng. Phys.* 2019; 71: 45-55.
- 291 14. Tannenbaum, C, Ellis RP, Eyssel F, Zou M, Schiebinger L. (2019). Sex and gender analysis
292 improves science and engineering. *Nature* 2019; 575: 137–146.
- 293 15. Kuehn BM. Getting to the heart of sex differences: growing evidence suggests women’s
294 heart disease is physiologically distinct. *Circulation* 2020; 141(14): 1198-1199.
- 295 16. Muskat JC, Rayz VL, Goergen CJ, Babbs CF. Hemodynamic modeling of the circle of
296 Willis reveals unanticipated functions during cardiovascular stress. *J. Appl. Physiol.* 2021;
297 131(3):1020-1034.
- 298 17. Cohrs NH, Petrou A, Loepfe M, Yliruka M, Schumacher CM, Kohll AX, Stark WJ. A soft
299 total artificial heart - first concept evaluation on a hybrid mock circulation. *Artif. Organs*
300 2017; 41(10): 948-958.
- 301 18. Rabineau J, Nonclercq A, Leiner T, Borne PVD, Migeotte PF, Haut B. Closed-loop
302 multiscale computational model of human blood circulation. Applications to
303 ballistocardiography. *Front. Physiol.* 2021; 2112.
- 304 19. Broomé M, Maksuti E, Bjällmark A, Frenckner B, Janerot-Sjöberg B. Closed-loop real-
305 time simulation model of hemodynamics and oxygen transport in the cardiovascular
306 system. *Biomed. Eng. Online* 2013; 12(1): 1-20.

- 307 20. Comunale G, Susin FM, Mynard JP. A female-specific cardiovascular lumped-parameter
308 model. 42nd Annual International Conference of the IEEE Engineering in Medicine &
309 Biology Society (EMBC) 2020; 2654-2657.
310 <https://ieeexplore.ieee.org/stamp/stamp.jsp?arnumber=9175427>
- 311 21. Comunale G. Lumped parameter models for congenital diseased and sex-specific
312 cardiovascular circulations. PhD Diss., University of Padova, Italy, 2020.
313 <https://hdl.handle.net/11577/3469095>
- 314 22. St. Pierre SR, Peirlinck M, Kuhl E. Sex matters: a comprehensive comparison of female
315 and male hearts. 2022; *Front. Physiol.* 13:831179.
- 316 23. De Vecchi A, Marlevi D, Nordsletten DA, Ntalas I, Leipsic J, Bapat V, Niederer SA. Left
317 ventricular outflow obstruction predicts increase in systolic pressure gradients and blood
318 residence time after transcatheter mitral valve replacement. *Sci. Rep.* 2018; 8(1), 1-11.
- 319 24. Gallo C, Olbers J, Ridolfi L, Scarsoglio S, Witt N. Testing a patient-specific in-silico model
320 to noninvasively estimate central blood pressure. *Cardiovas. Eng. Techn.* 2021; 12(2): 144-
321 157.
- 322 25. Cuomo F, Ferruzzi J, Agarwal P, Li C, Zhuang ZW, Humphrey JD, Figueroa CA. Sex-
323 dependent differences in central artery haemodynamics in normal and fibulin-5 deficient
324 mice: implications for ageing. *Proc. R. Soc. A.* 2019; 475:20180076.
- 325 26. Corsini C, Cervi E, Migliavacca F, Schievano S, Hsia TY, Pennati G. Mathematical
326 modelling of the maternal cardiovascular system in the three stages of pregnancy. *Med.*
327 *Eng. Phys.* 2017; 47: 55-63.
- 328 27. Pekkan K, Erturk H, Culha MG, Serefoglu EC. A Patient-Specific Lumped Parameter
329 Model of Human Penile Erection. *J. Sex. Med.* 2017; 14(1): S128.
- 330 28. Ng WK, Ng EYK, Chia SJ. The engineering analysis of bioheat equation and penile
331 hemodynamic relationships in the diagnosis of erectile dysfunction: part I -theoretical
332 study and mathematical modeling. *Int. J. Impot. Res.* 2008; 20(3), 295-306.
- 333 29. Comunale G, Susin FM, Mynard JP. Ventricular wall stress and wall shear stress
334 homeostasis predicts cardiac remodeling during pregnancy: a modeling study. *Int. J. Num.*
335 *Meth. Bio. Eng.* 2022; 38(1): e3536.
- 336 30. Gleason, R. L., & Sedaghati, F. A mathematical model of maternal vascular growth and
337 remodeling and changes in maternal hemodynamics in uncomplicated pregnancy.
338 *Biomech. Model. Mechan.* 2022; 21(2): 647-669.
- 339 31. Carson J, Warrander L, Johnstone E, van Loon R. Personalising cardiovascular network
340 models in pregnancy: a two-tiered parameter estimation approach. *Int. J. Num. Meth. Bio.*
341 *Eng.* 2021; 37(11): e3267.
- 342 32. Li Z, Chen Y, Zeng X, Stephen S, Li Y, Li H, Fan H. Clinical and hemodynamic insights
343 into the use of internal iliac artery balloon occlusion as a prophylactic technique for treating
344 postpartum hemorrhage. *J. Biomech.* 2021; 129:110827.
- 345 33. Ordoñez MV, Biglino G, Caputo M, Curtis SL. Pregnancy in the FONTAN palliation:
346 physiology, management and new insights from bioengineering. *J. Cong. Cardiol.* 2021;
347 5(1): 1-10.
- 348 34. Díaz-Navarro R. Takotsubo syndrome: the broken-heart syndrome. *Br. J. Cardiol.* 2021;
349 28(1): 30-4.

350
351 Francesca Maria Susin
352 Cardiovascular Fluid Dynamics Laboratory – Department of Civil, Environmental and Architectural
353 Engineering, University of Padova
354 Via Marzolo 9 – 35131 Padova, Italy
355 Phone: +39 049 8275443
356 Fax: +39 049 8275446
357 Email: francescamaria.susin@unipd.it